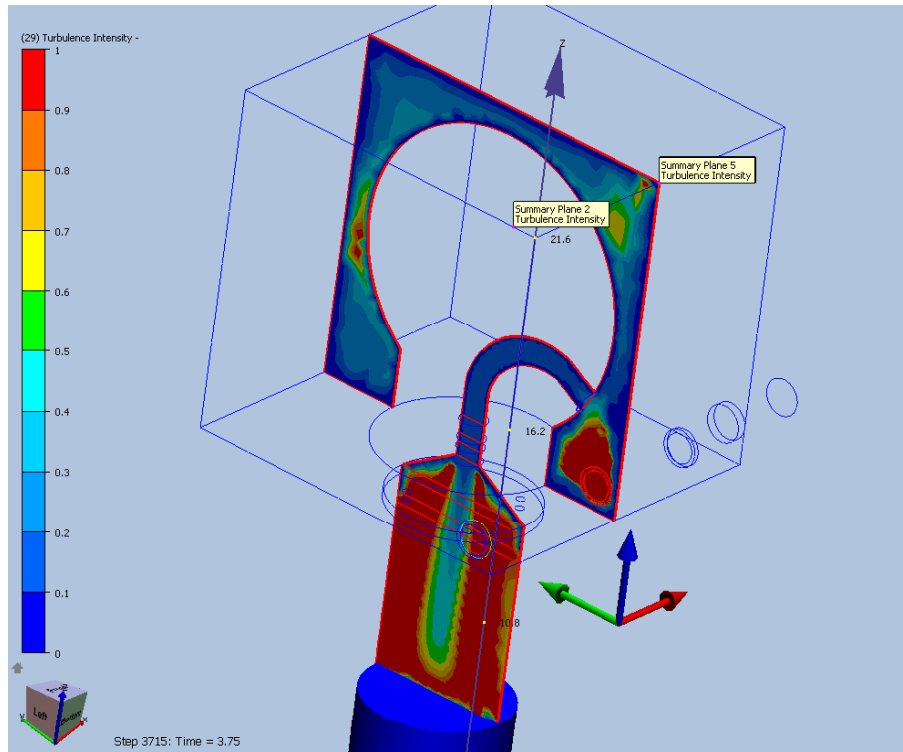


Life Support Helmet CO₂ Transport Modeling



Key Performers:

Dr. John Camperman, NSWC-PCD

Robert Hughes, NSWC-PCD

Dr. Rick Smith, NSWC-PCD

Objectives:

- Investigate CFD helmet CO₂ mixing-transport models.
- Validate CFD models relative to experimental research.
- Explore minimizing CO₂ with minimal flow and power.

Technical Challenges:

- Multi-species flow.
- Laminar and turbulent flow interaction.
- Eddy and molecular diffusion.
- Harmonic problem with relaminarization.

Technical Approach:

- Refine finite difference harmonic mixing zone model.
- Develop inhalation and exhalation steady flow CFD models and correlate CFD results with previous experimental data.
- Develop dynamic breath cycle CFD model and optimize, validate it using experimental data.

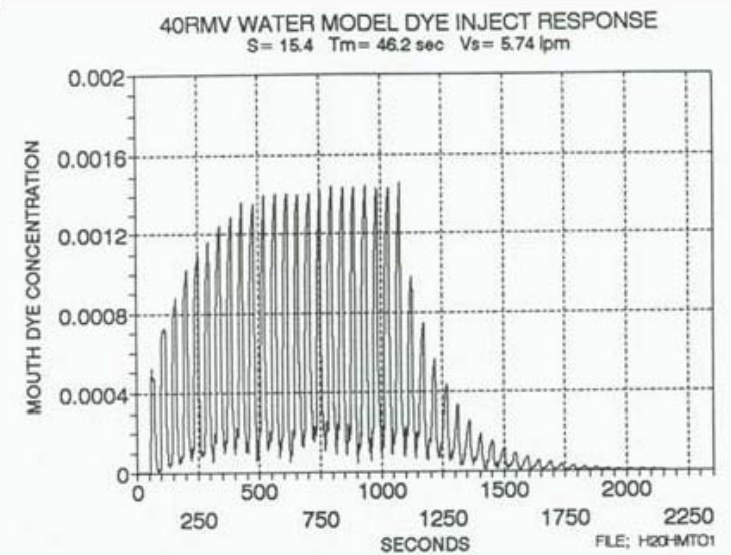
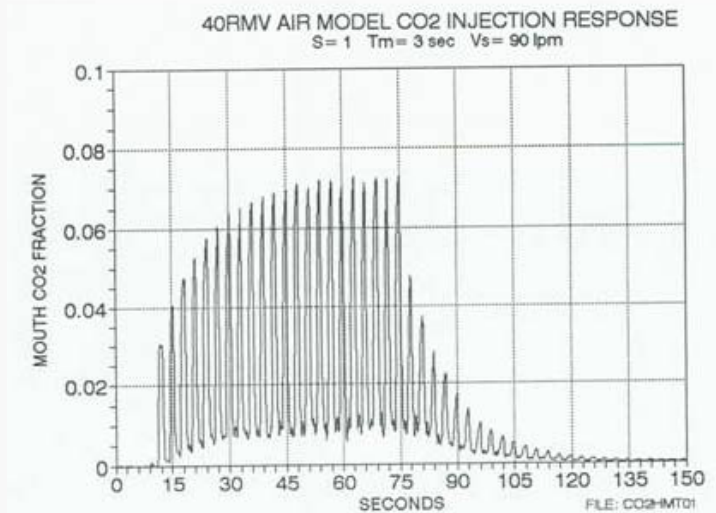
S&T Products:

- Assessment of CFD validity for helmet CO₂ transport.
- Investigation of modeling techniques for potential helmet improvements applicable to diving, firefighting, CBRN protection, and aerospace life support helmets.

PROBLEM

- ❑ Traditional well mixed assumptions require over 150 liters/min fresh gas flow to maintain average inhaled CO_2 below 2% at one atmosphere.
- ❑ High flow generates noise, and consumes excessive gas or blower power.
- ❑ Oral-nasal masks control CO_2 but are not desirable.

Previous Experimental Modeling



TWO CYCLE COMPLETE MIXING

Inhale
$$\dot{F}_{hi} + F_{hi} \frac{\dot{V}_s}{V_h} = F_s \frac{\dot{V}_s}{V_h}$$

Exhale
$$\dot{F}_{he} + F_{he} \left(\frac{\dot{V}_s - \dot{V}_{be}}{V_h} \right) + F_e \frac{\dot{V}_{be}}{V_h} = F_s \frac{\dot{V}_s}{V_h}$$

Boundary
Conditions
(coupling)

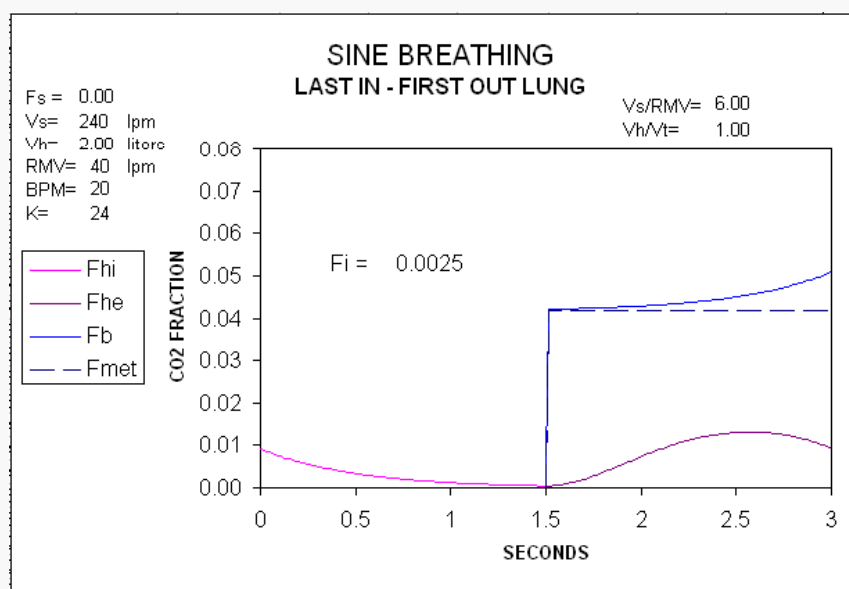
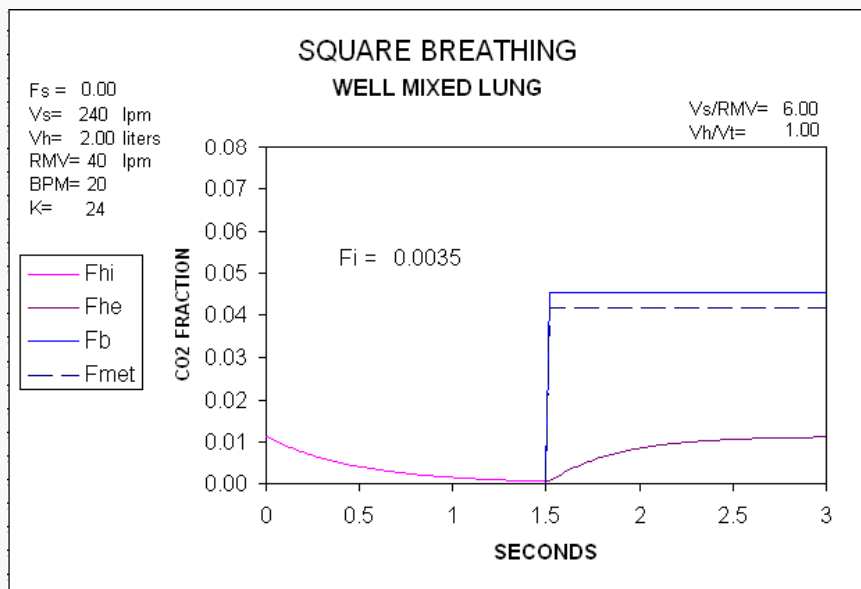
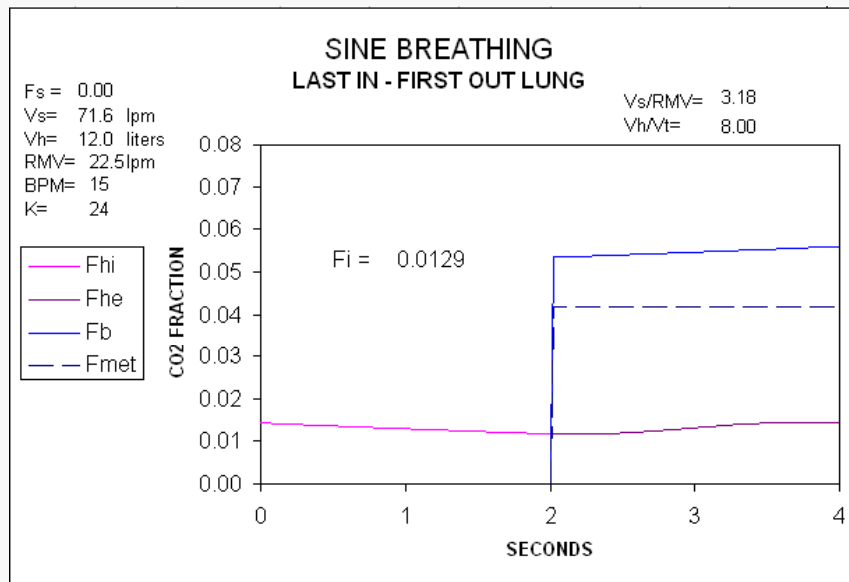
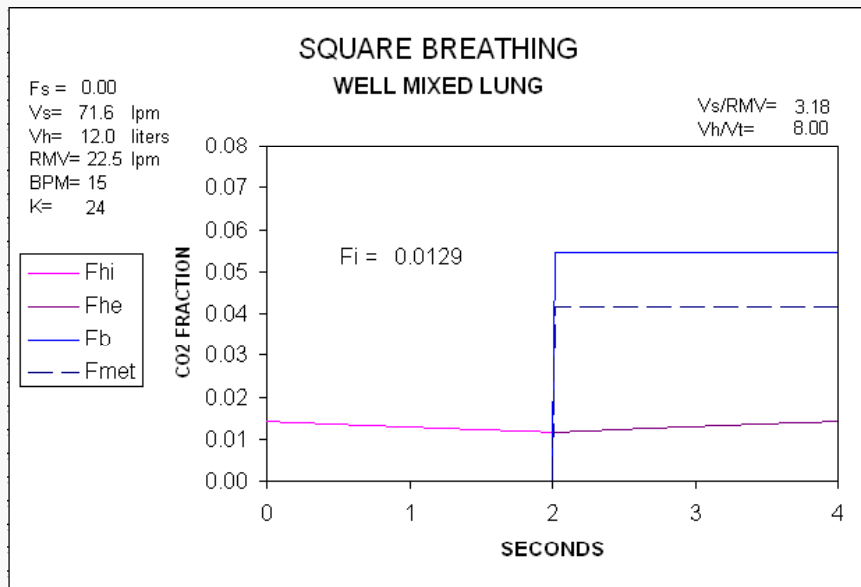
$$F_{hi}(O) = F_{he}(T)$$

$$F_{hi}(T_i) = F_{he}(T_i)$$

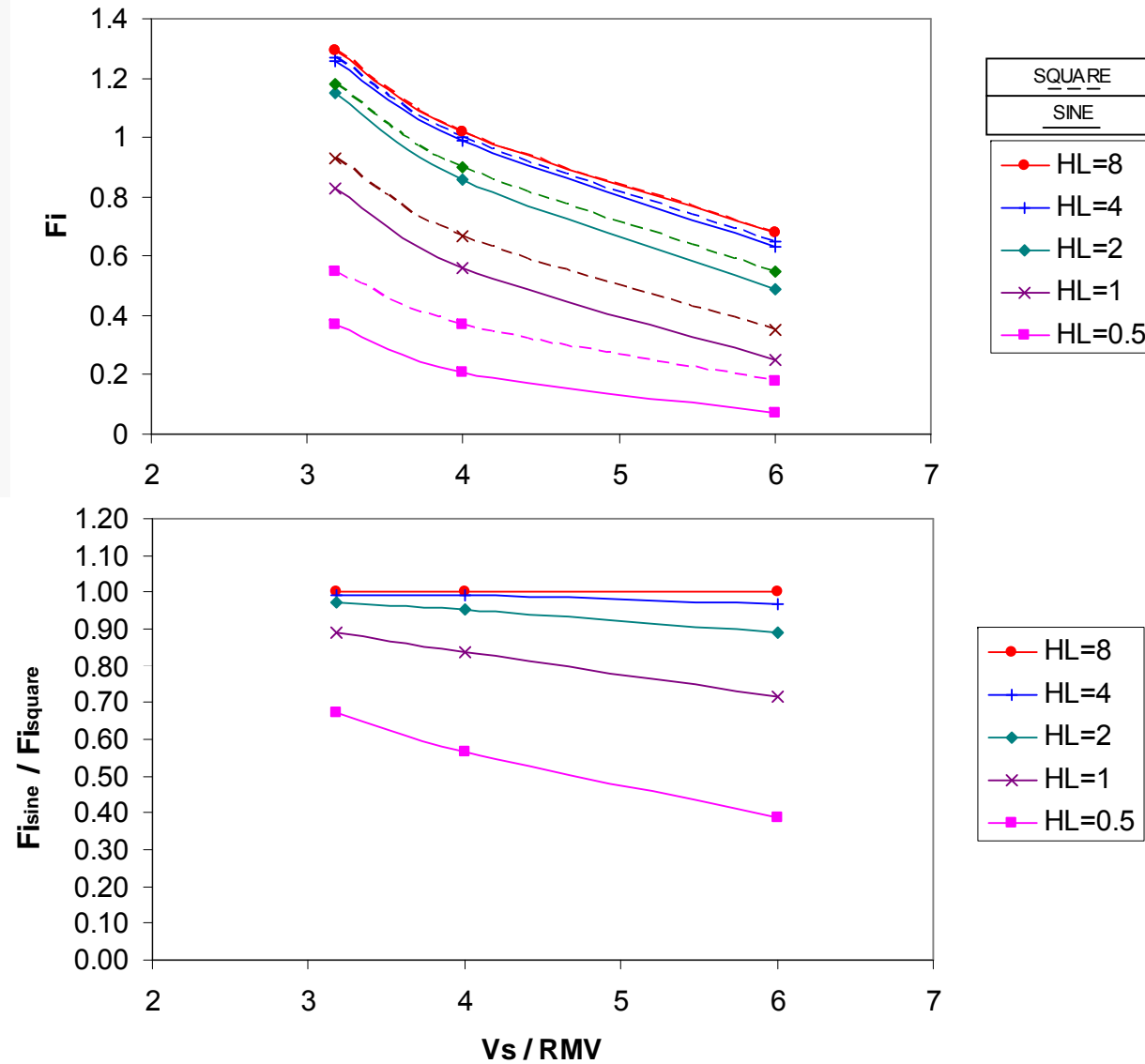
Respiratory
CO₂
$$-\int_{T_i}^T F_e \dot{V}_{be} dt = \int_0^{T_i} F_{hi} \dot{V}_b dt + \dot{V}_{CO_2} T$$

Average inhaled
CO₂ fraction

$$F_i = \frac{1}{V_t} \int_0^{T_i} F_{hi} \dot{V}_{bi} dt$$

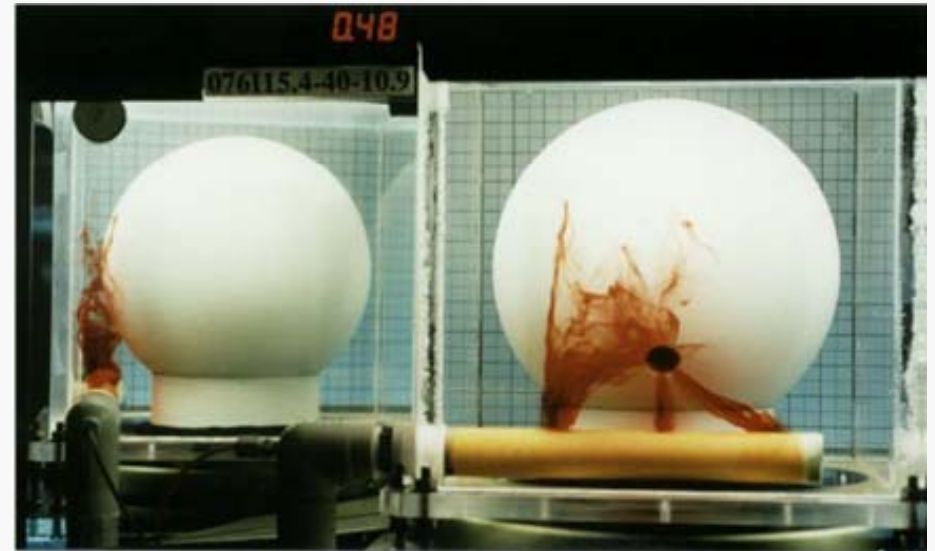
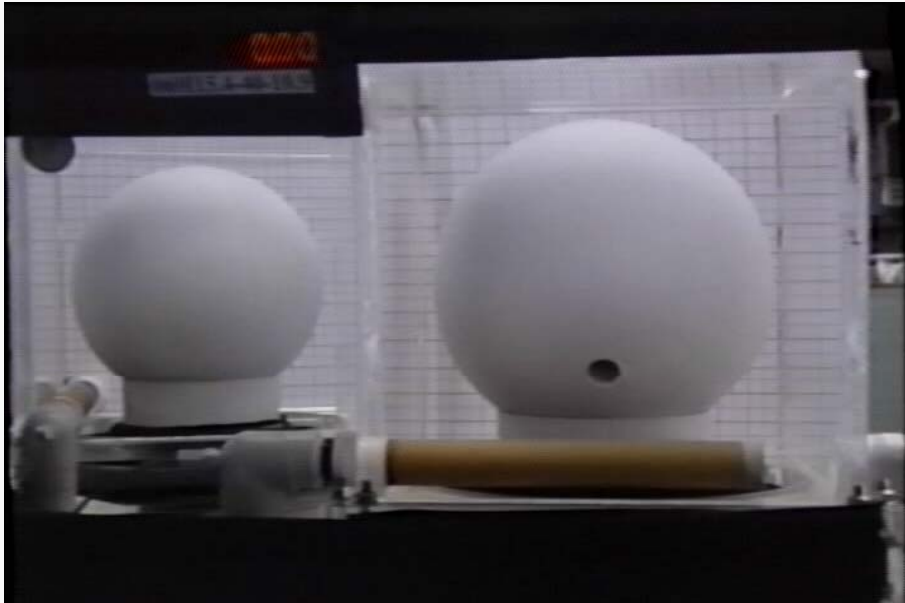


HELMET TWO CYCLE COMPLETE MIXING Square and Sinusoidal Breathing Inspiratory CO₂ (Finite Difference Model)

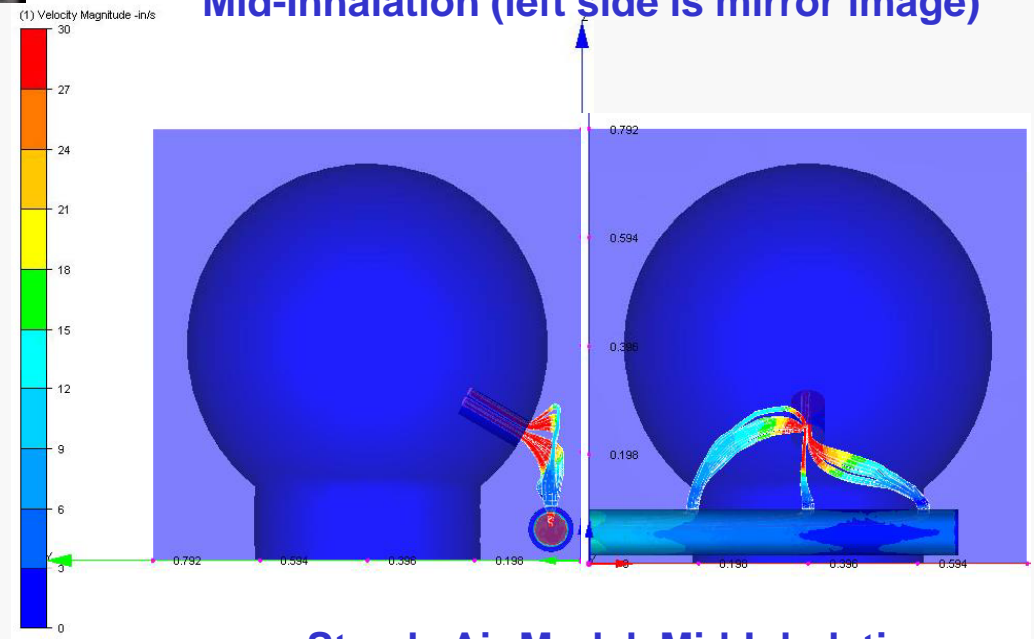


40 RMV Inhalation Streak Lines and Particle Traces

Breath: Supply (lpm) Air 126:170; Water 8.1:10.9



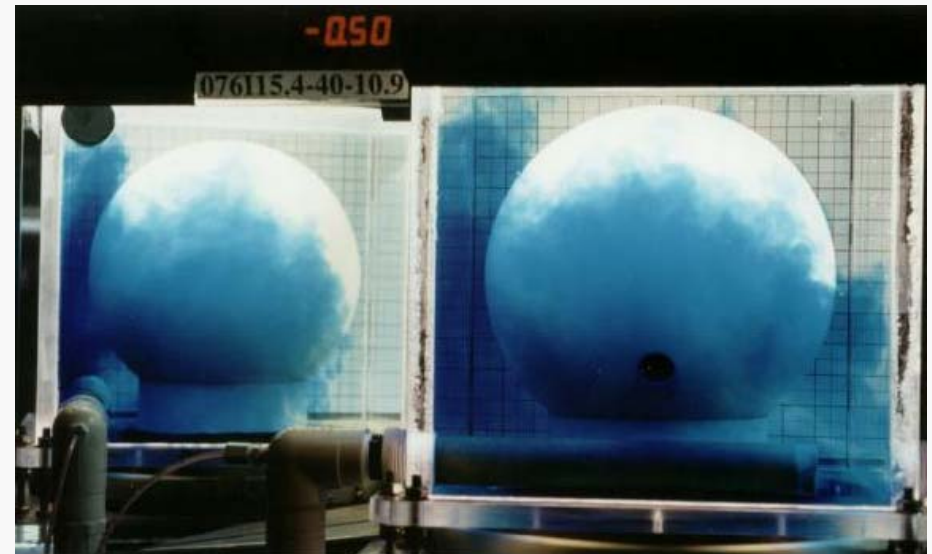
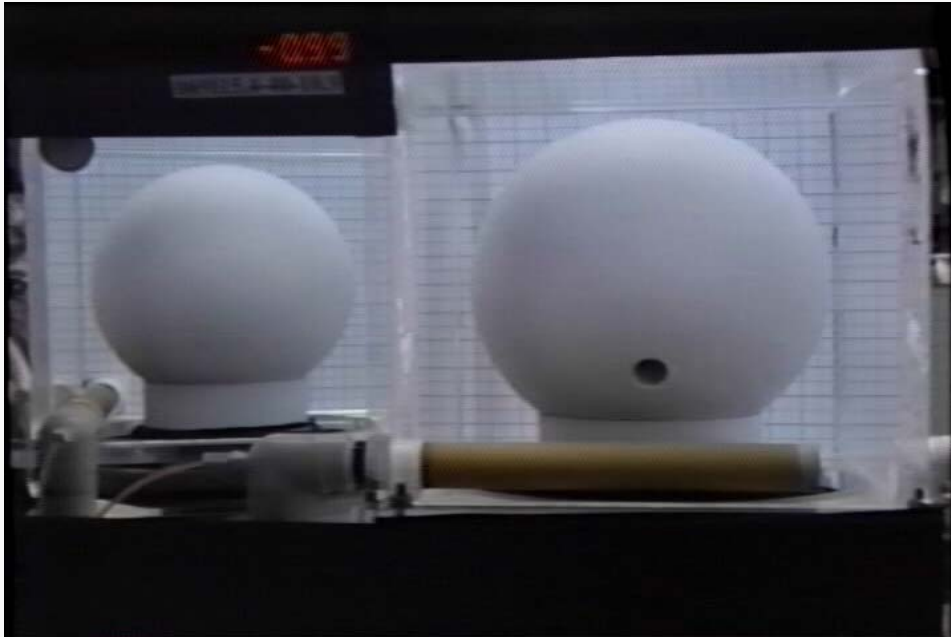
Mid-Inhalation (left side is mirror image)



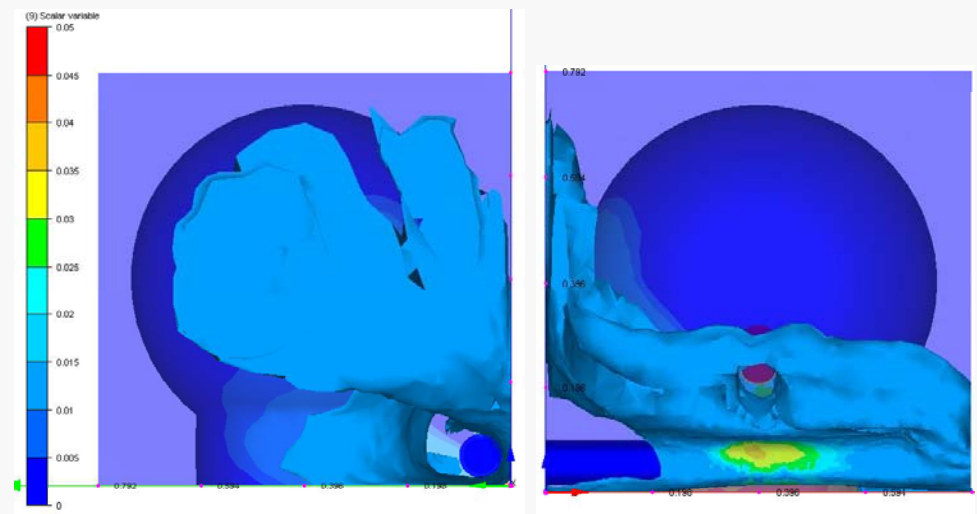
Steady Air Model, Mid-Inhalation

40 RMV Exhalation Breath Plumes

Breath: Supply (lpm) Air 126:170; Water 8.1:10.9



Mid-Exhalation (left side is mirror image)

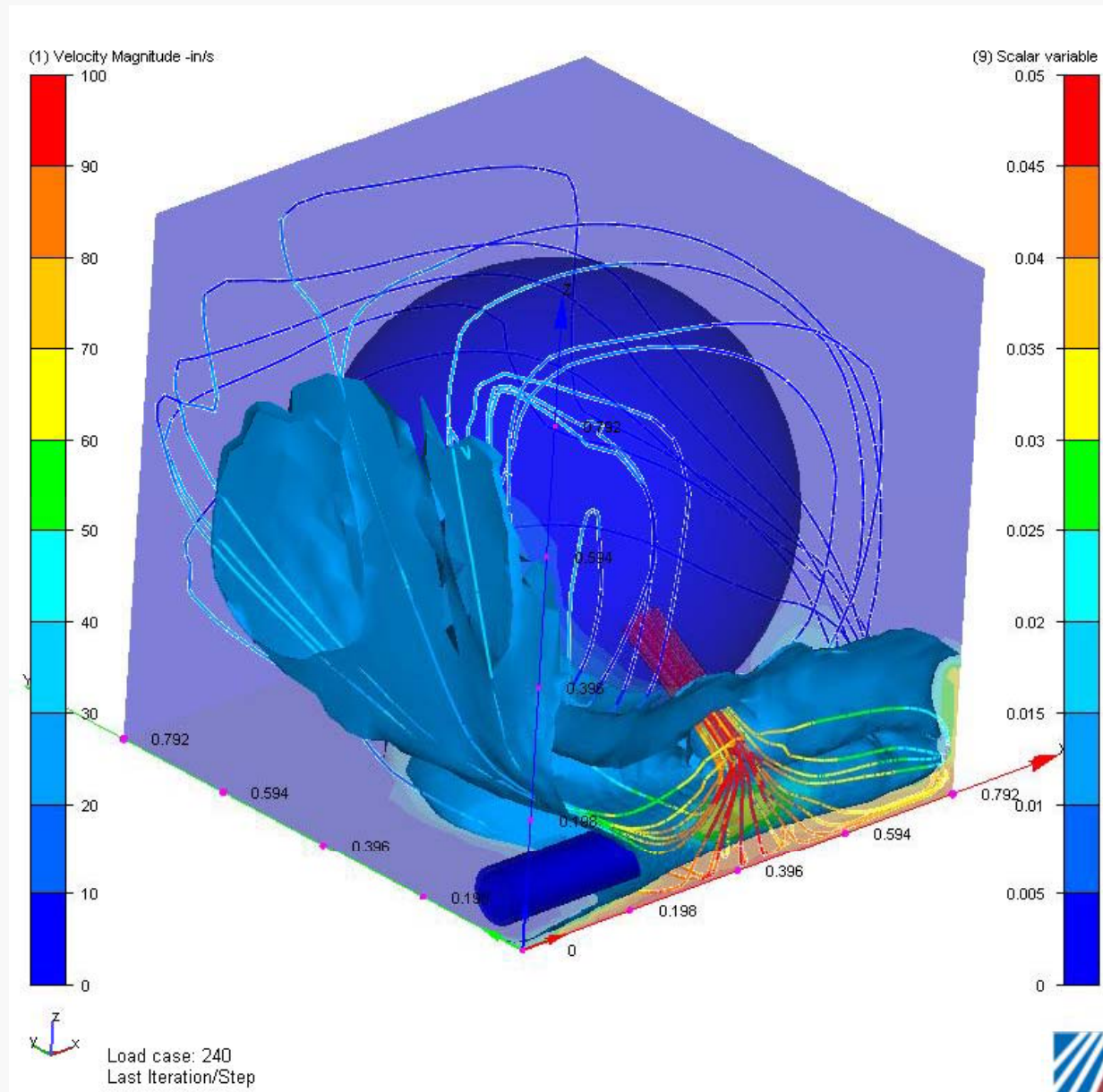


Steady Air Model, Mid-Exhalation
0.015 CO₂ Concentration Surface

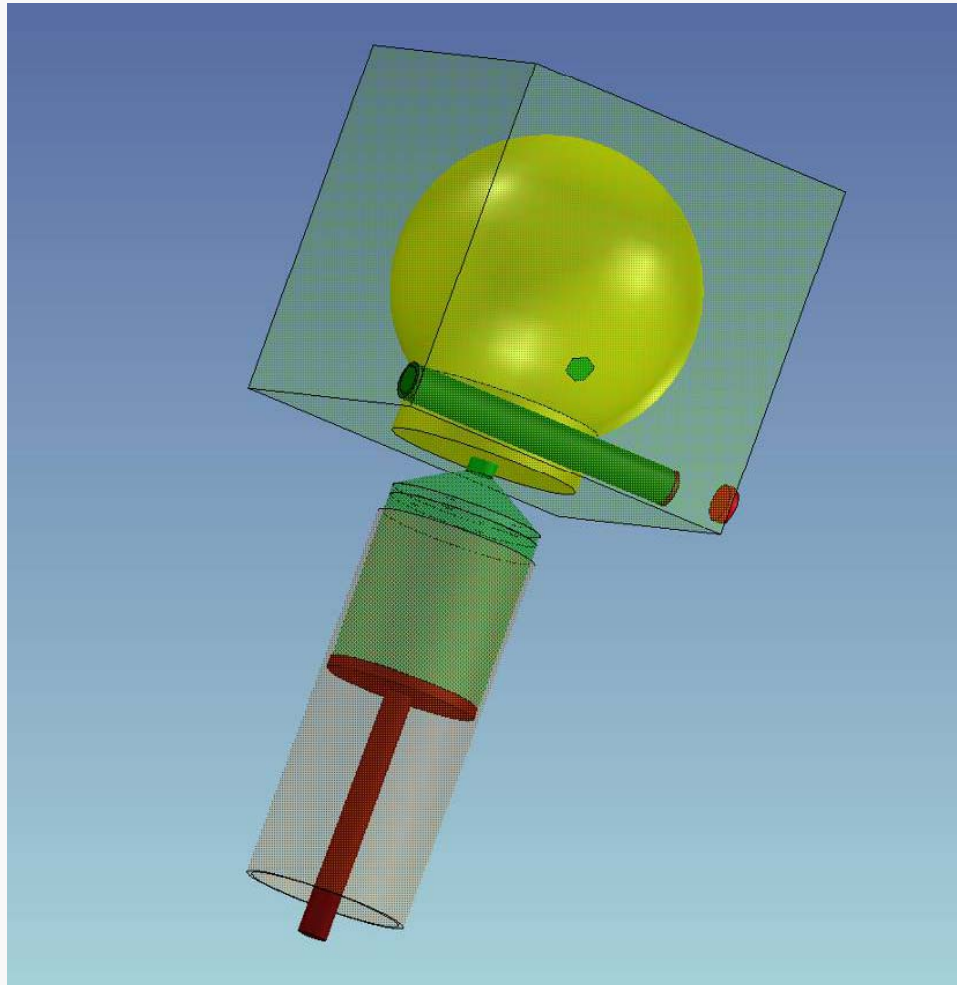
40 RMV Mid-Exhalation Steady Air Model

Breath: 126 lpm Supply: 170 lpm

Particle Traces
and
0.015 CO₂
Concentration
Surface

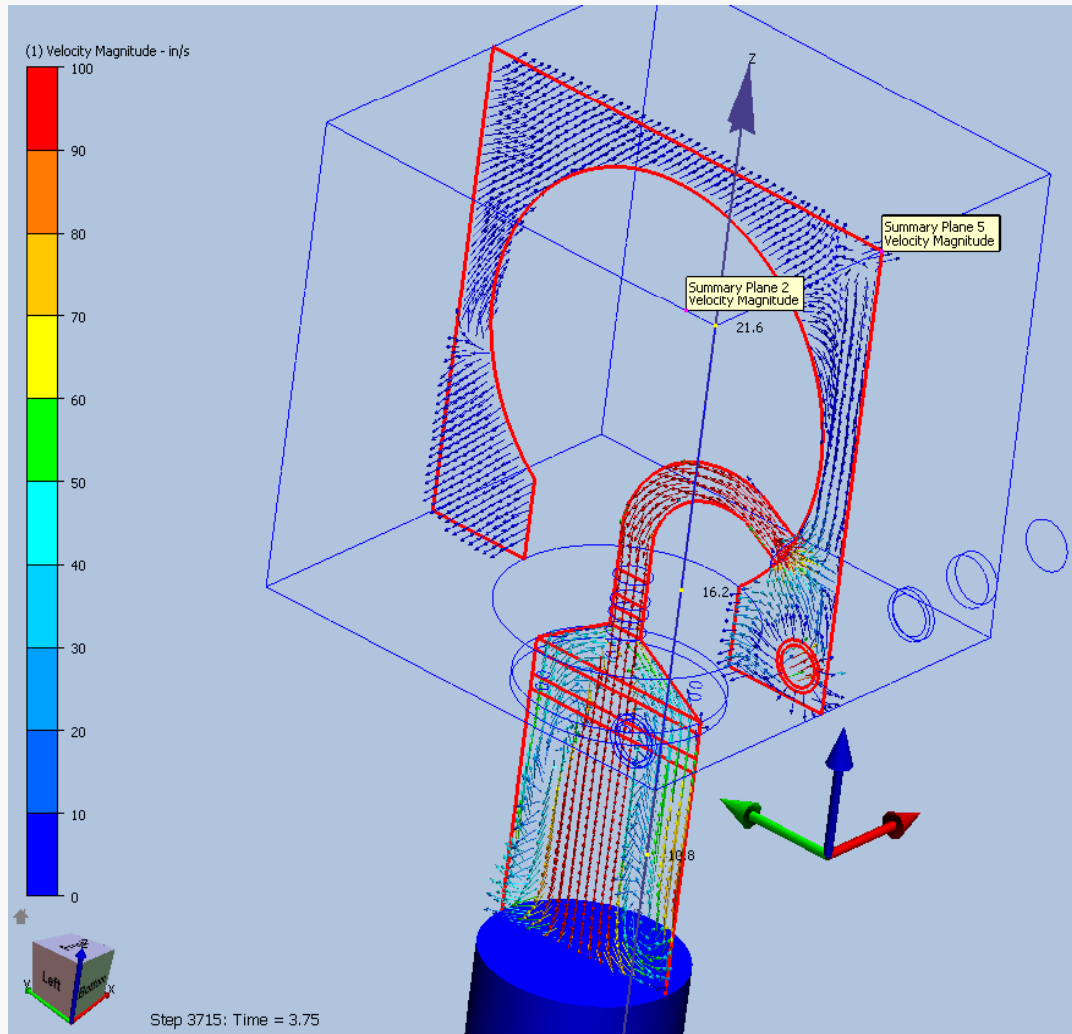


Helmet-Lung Harmonic Air Model Geometry

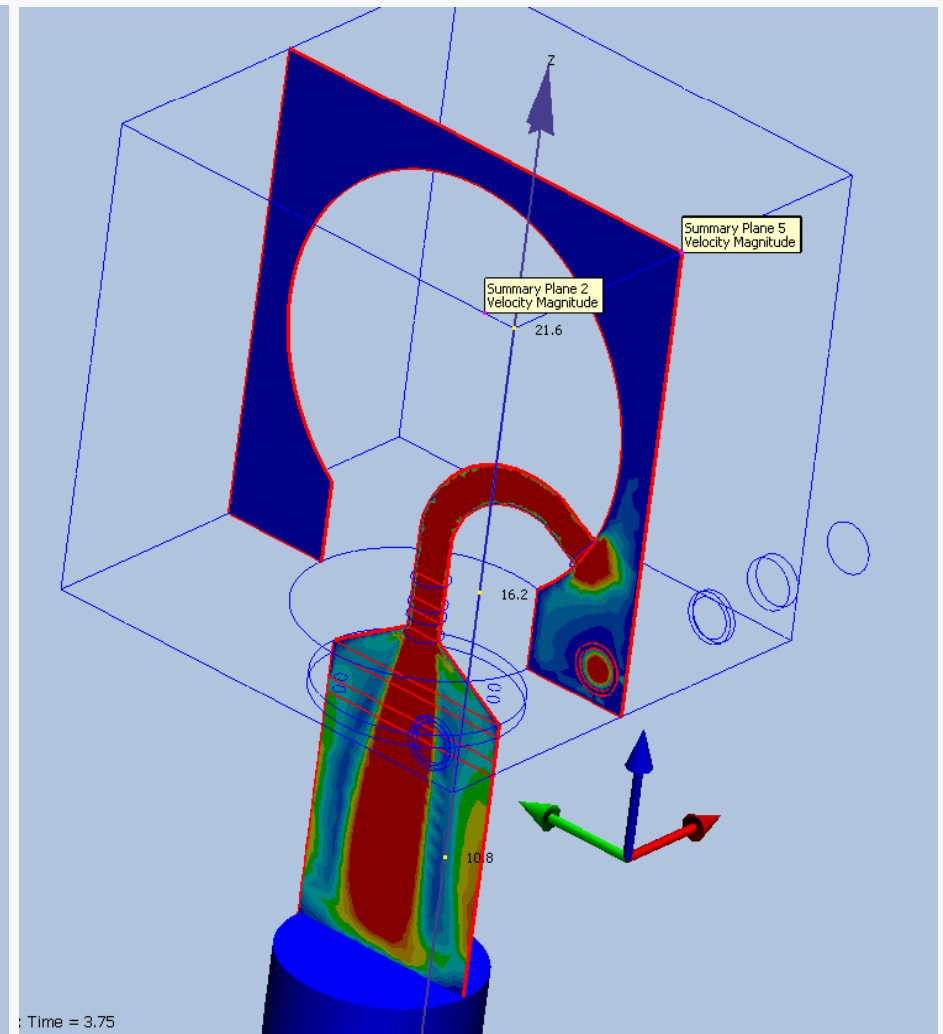


Mid-Inhalation Square Wave Air Model

Breath: ≈ 126 lpm Supply: 170 lpm



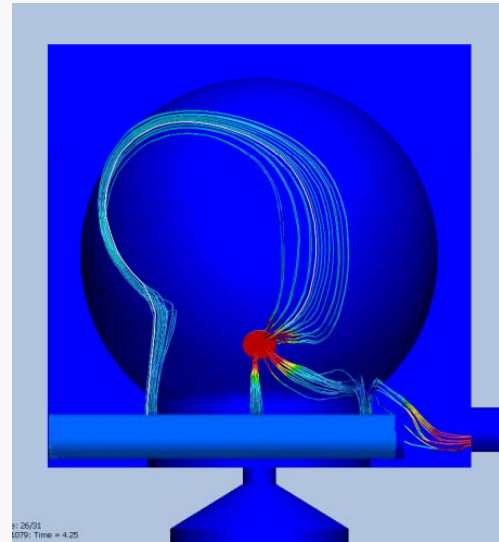
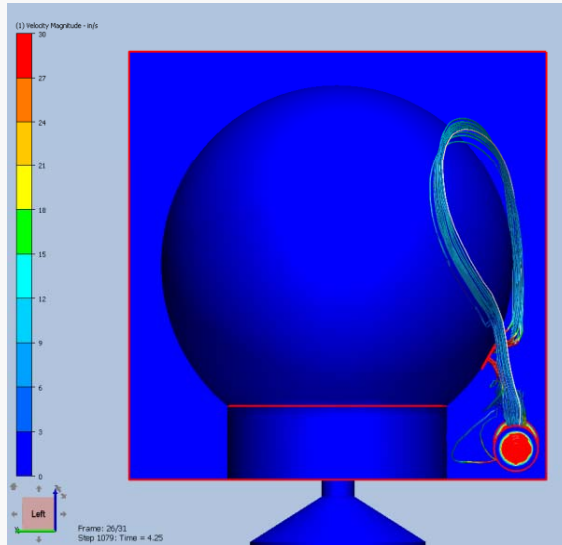
3D velocity vectors; fixed length, color magnitude.



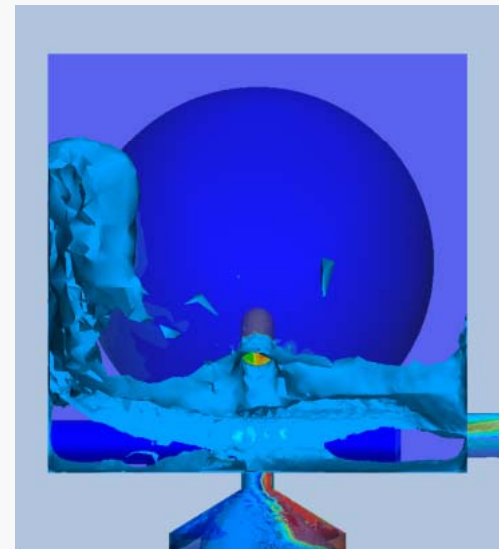
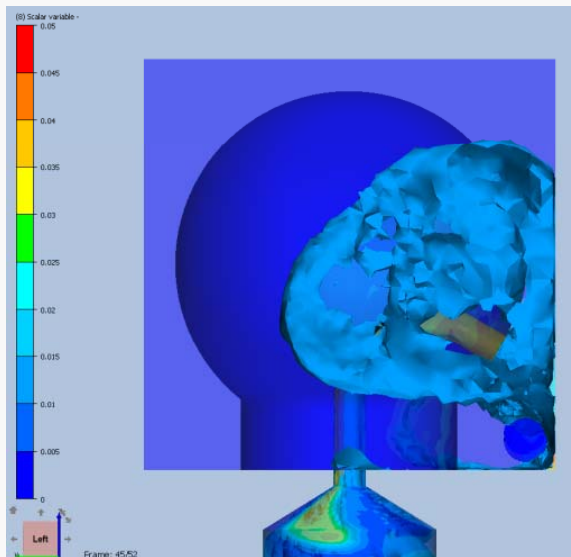
Velocity contours.

40 RMV Mid-Inhalation Harmonic Air Models

Breath: 126 lpm Supply: 170 lpm



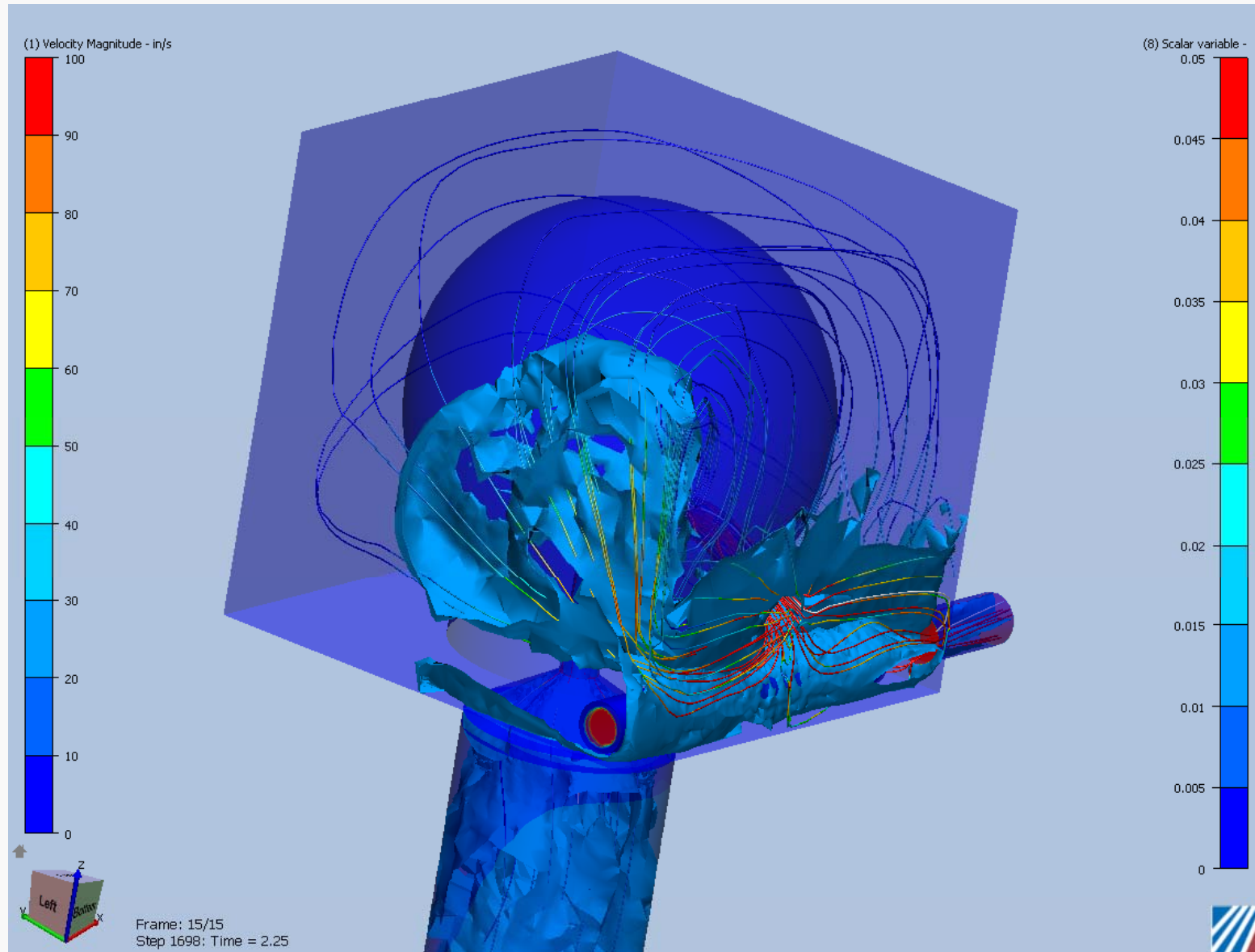
**Square Wave Air Model
Mid-Inhalation**



**Sinusoidal Air Model
Mid-Exhalation**

40 RMV Mid-Exhalation Sinusoidal Air Model

Breath: 126 lpm Supply: 170 lpm





FINDINGS

- Finite difference complete mixing model indicates inhaled CO₂ fraction is greatly reduced with sine breathing versus square breathing for small mixing volumes.
- Steady flow CFD simulations represent fundamental harmonic peak flow behaviors.
- Harmonic CFD simulations may be used to model helmet harmonic flows.



APPLICATIONS



Modeling techniques may guide innovative helmet design geometries that optimize CO₂ transport.

- Navy Flyaway Mixed Gas semi-closed circuit rebreather interface.
- Powered Air Purifying Respirators
- NASA Space Suit Systems